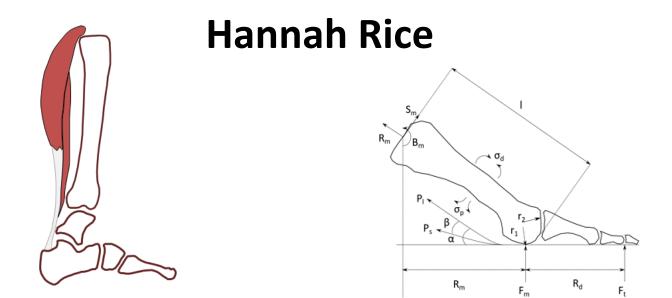
Estimating bone loading during physical activity: where do we go next?





10th International Conference on Sport Sciences Research and Technology Support



Estimating bone loading during physical activity: where do we go next?

- Bone stress injuries
- Identification of risk factors
- Internal loading
- Participant-specificity
- Real-time and real-world
- Validation







Running Overuse Injuries

- Overall incidence 19% 79% ¹
- 2.5 33.0 injuries per 1000 hours of running²
- Bone stress injuries can be particularly problematic:
 - several months of time loss³
 - recurrence ^{4,5}

1. Van Gent et al., 2007; 2. Videbæk et a., 2015; 3. Wood et al., 2014; 4. Milgrom et al., 1985, Giladi et al., 1986 1,2, Retrieved from Willwacher et al., 2022



Bone Stress Injuries

- Bone stress injuries are a continuum of injuries ¹ from bony microfracture to visible cortex fracture
- Stress fractures are the most serious
- up to 30% of running-related injuries ²

Bone Stress Injuries

- tibia is the most common site of stress injury ¹
- followed by second and third metatarsals ^{2,3,4,5}

1. Wood et al., 2014; 2. Bennell et al., 1996; 3. Fetzer & Wright, 2006; 4. Gross & Bunch, 1989; 5. Iwamoto & Takeda, 2003.



Bone Stress Injuries

- Repetitive loading can lead to microdamage accumulation ^{1,2}
- This is a normal response to bone loading and can be beneficial ³
- But excessive accumulation can impair bone properties ⁴, and increase SF risk ⁵.
- 1. Burr et al., 1997; 2. Warden et al., 2014; 3. Frost, 1994; 4. Burr et al., 1998; 5. Burr et al., 2011

Identifying risk factors for bone stress injury

What can we do?









Prospective study of injury in Royal Marines recruits

Nunns et al., 2016; Rice at al., 2017; Dixon et al., 2019



Injuries by site in RM recruits (% of all injuries):

MSF = 11.4% TSF = 8.3%

Median recovery time:

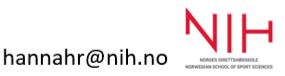
MSF = 32.5 weeks TSF = 23 weeks

Prospective study of injury in Royal Marines recruits



- 1065 male recruits
- 32 week training programme

Aim: to identify biomechanical gait characteristics during barefoot running that may be associated with increased risk of a lower limb injury during Royal Marines training.



Prospective study of injury in Royal Marines recruits



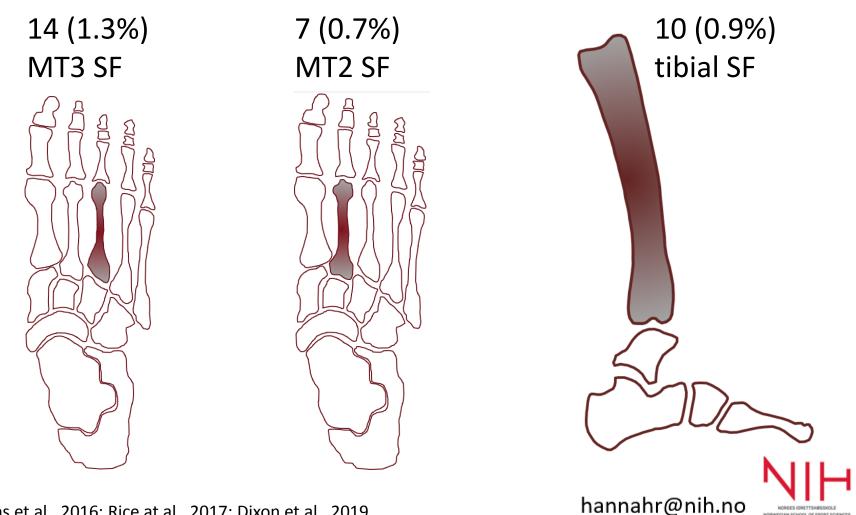
- anthropometrics
- kinematics
- plantar pressure
- passive range of motion
- barefoot running at 3.6 m.s⁻¹



Nunns et al., 2016; Rice at al., 2017; Dixon et al., 2019

Injury Outcomes

419 (39.3%) completed training at the first attempt injury-free



Nunns et al., 2016; Rice at al., 2017; Dixon et al., 2019

Tibial stress fracture

Four variables associated with increased risk of TSF

- 🔸 BMI
- \downarrow Bimalleolar breadth
- \downarrow Tibial rotation
- 个 Peak heel pressure





Tibial stress fracture

Lower BMI associated with increased risk one unit \downarrow associated with 79% \uparrow risk

Lower bimalleolar breadth associated with increased risk one mm \downarrow associated with 37% \uparrow risk





Tibial stress fracture

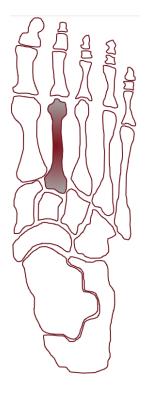
Lower tibial internal rotation ROM associated with increased risk 1°↓ associated with 28% ↑ risk

Greater peak heel pressure associated with increased risk $1 \text{ N.cm}^{-2} \uparrow \text{ associated with } 25\% \uparrow \text{ risk}$





Challenges with approach of identifying risk factors

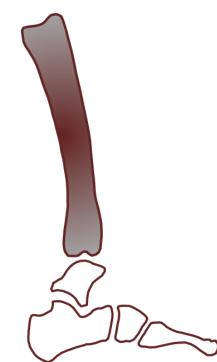


Sample size requirements

Injury mechanisms for different sites

Retrospective study design

Focus on single variables

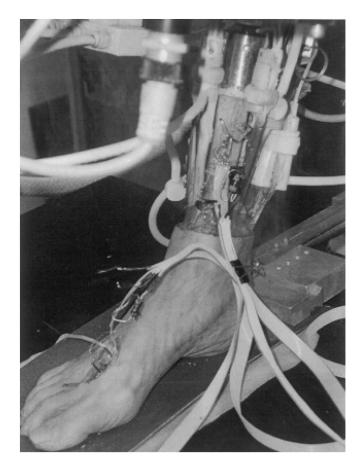




What is happening internally?

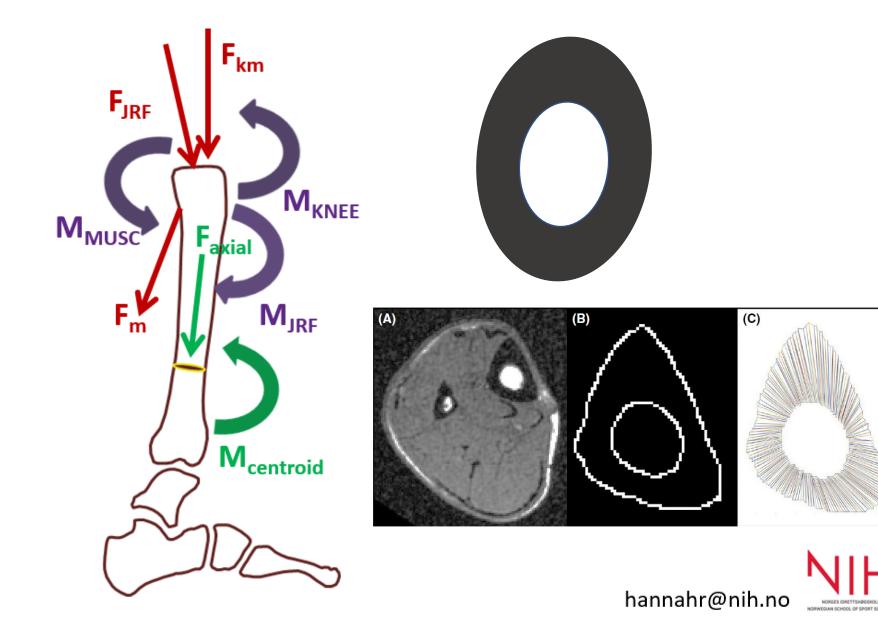
External vs internal loading



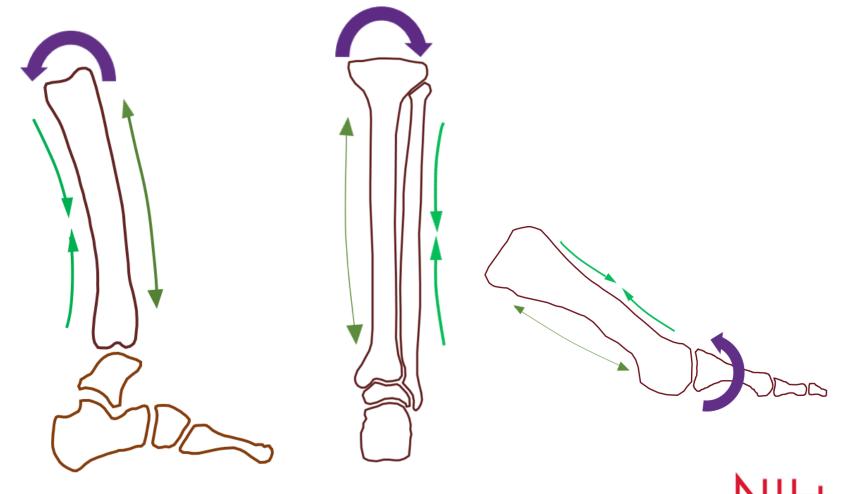




Modelling approaches



What happens when we load the long bones?



Tibial stress estimates during running



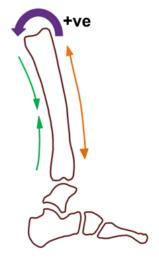
SCANDINAVIAN JOURNAL OF MEDICINE & SCIENCE IN SPORTS

ORIGINAL ARTICLE | 🔂 Open Access | 💿 🚺

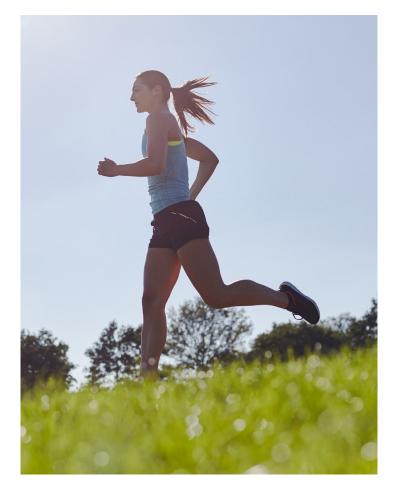
Tibial stress during running following a repeated calf-raise protocol

Hannah M. Rice 🔀, Megan Kenny, Matthew A. Ellison, Jon Fulford, Stacey A. Meardon, Timothy R. Derrick, Joseph Hamill

Medicine & Science Sports & Exercise







Rice, Mai,...Willwacher (under review)

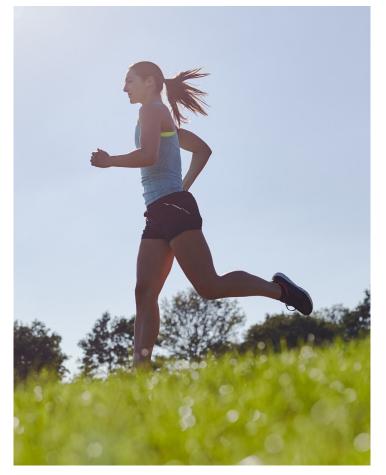
Aim: to quantify tibial bending moments and stress when running at different speeds on surfaces of different gradients





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Rice, Mai,...Willwacher (under review)

20 recreational runners (male and female)

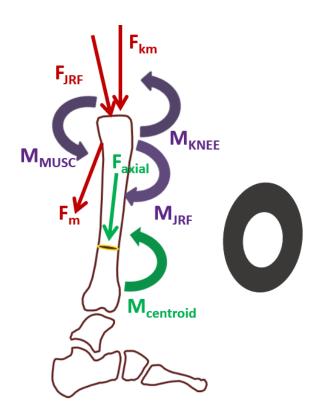
- Ran at 3 speeds (2.5 m.s⁻¹, 3.0 m.s⁻¹, 3.5 m.s⁻¹)
- On different gradients (level: 0%;
- ±5%, ± 10%, ± 15%)





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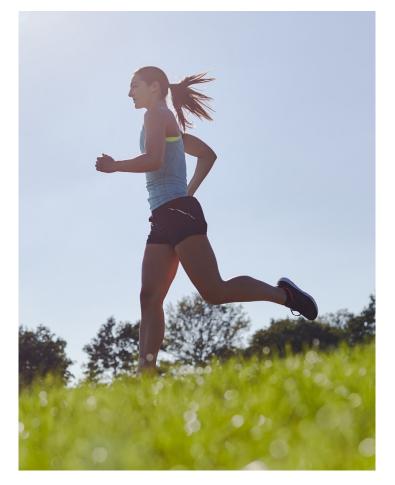
Rice, Mai,...Willwacher (under review)

- Synchronised kinematic and kinetic data collected
- Bending moments at distal 1/3 tibia
- 2-way repeated measures ANOVA
- ROI SPM analysis from 10% 90% of stance









Rice, Mai,...Willwacher (under review)

Results

Peak MBE:

- No interaction effect
- Main effect for running speed
- Main effect for gradient

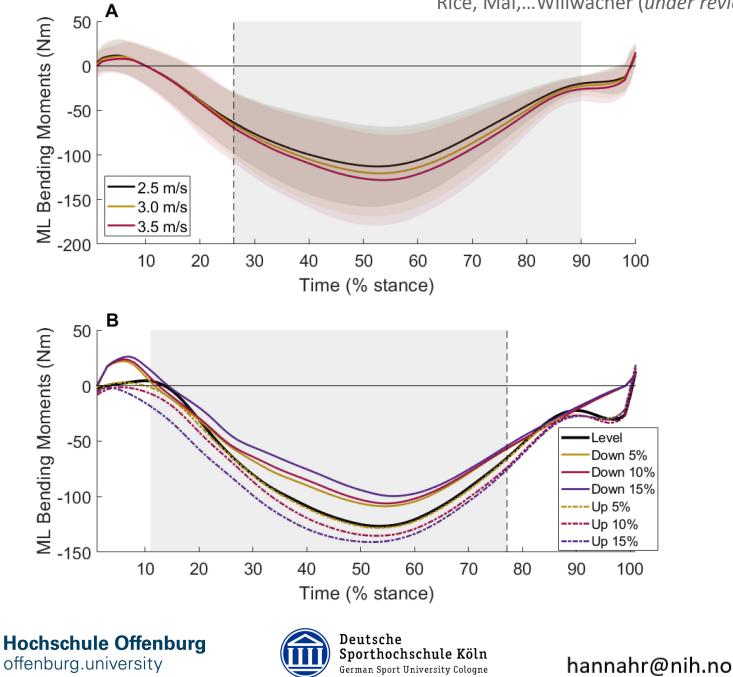




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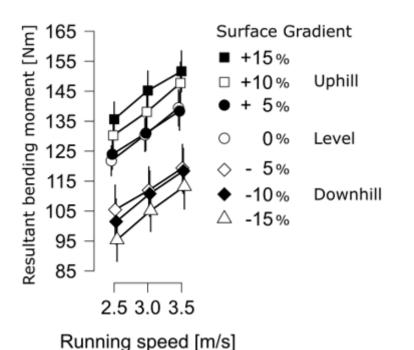






Rice, Mai,...Willwacher (under review)

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Rice, Mai,...Willwacher (under review)

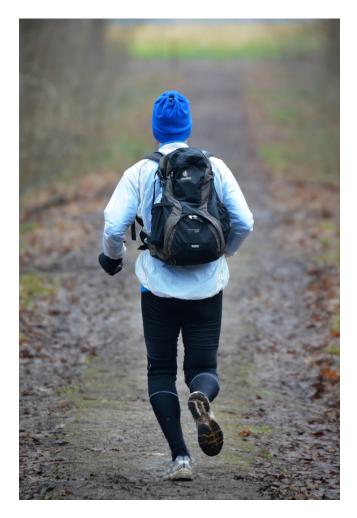
- Running at faster speeds and uphill on gradients ≥+10% increased internal tibial loading
- Slower running and downhill running reduced internal loading

Adapting running speed according to the gradient could be a protective mechanism









Aim: to quantify the effects of running at a faster speed and with increased weight on tibial loading

Population: 14 male distance runners, running at least 40 km/week



Rice, Seynnes,..., Werkhausen (in preparation)

Protocol: Barefoot running

Preferred speed, + 20% preferred speed 3.1 \pm 0.3 m.s⁻¹, 3.7 \pm 0.3 m.s⁻¹

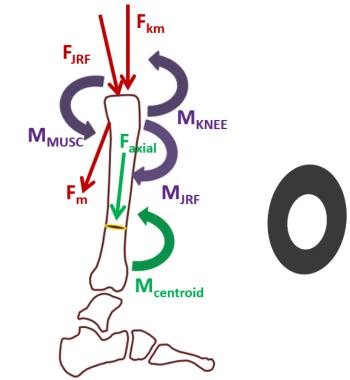
with and without +20% of body weight

Synchronised kinematic and kinetic data collected



• 2-way repeated measures ANOVA

 ROI SPM analysis from 10% – 90% of stance





Rice, Seynnes,..., Werkhausen (in preparation)

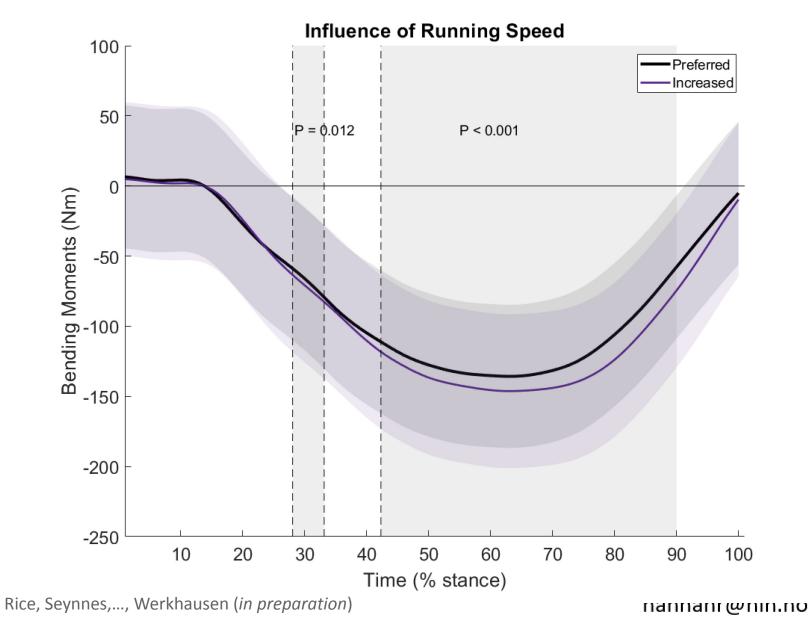
SPM Results

No interaction effect (p > 0.05)

hannahr@nih.no

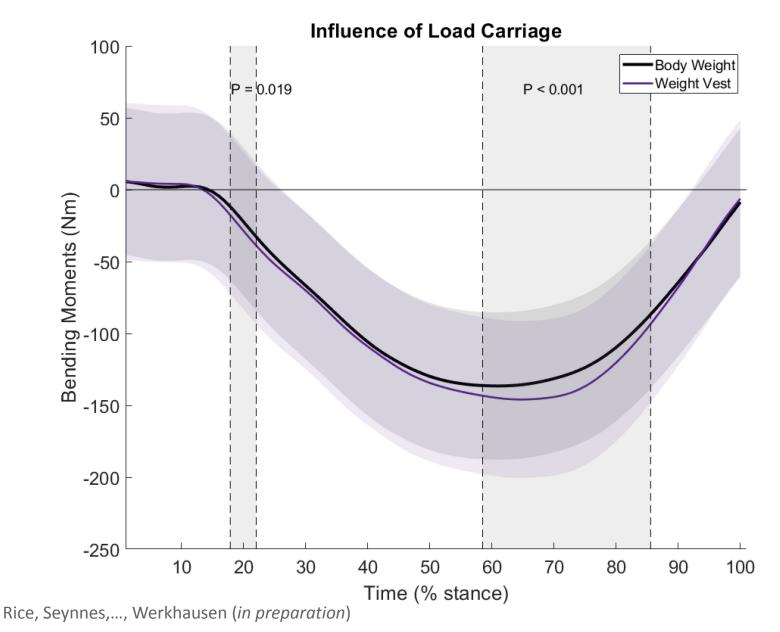
Rice, Seynnes,..., Werkhausen (in preparation)

Main effect for running speed

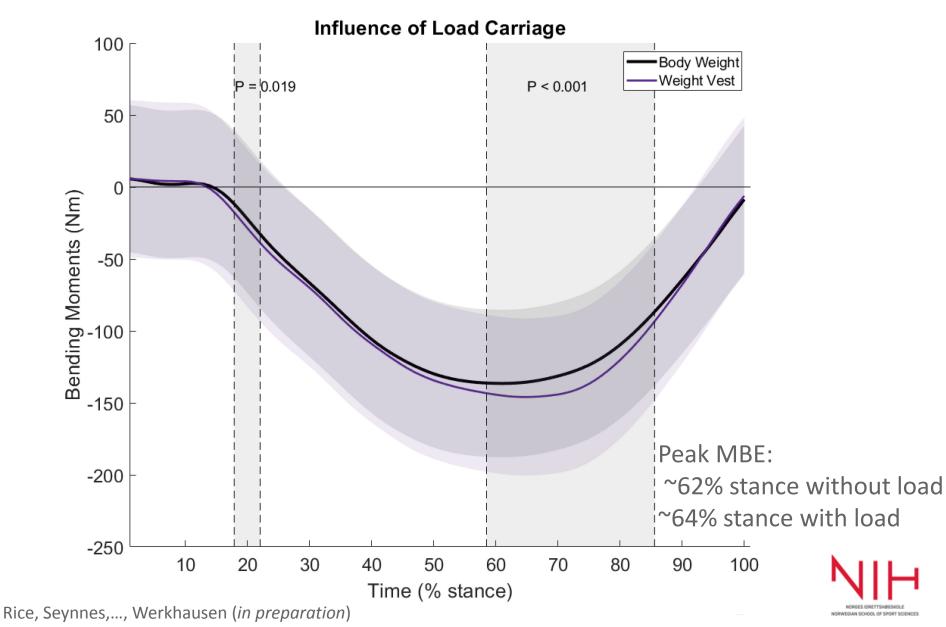


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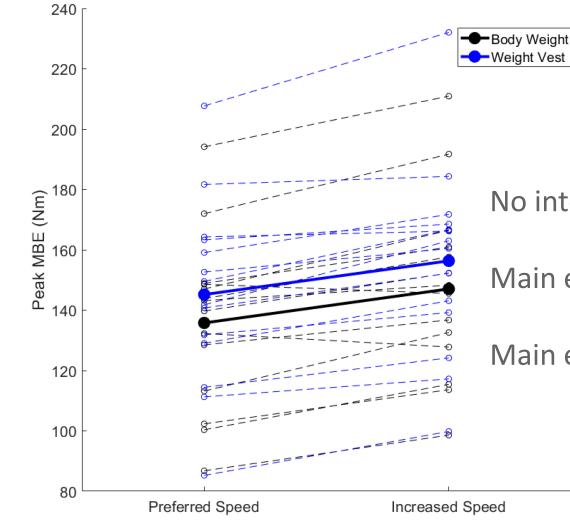
Main effect for added weight



Main effect for added weight



Discrete Results - Peak Bending Moment



No interaction effect (p = 0.967)

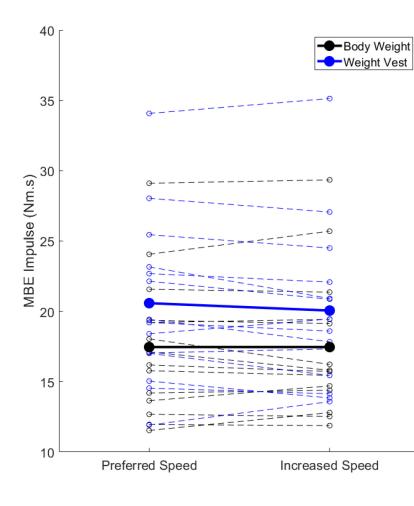
Main effect for speed (p < 0.001)

Main effect for weight (p < 0.001)



Rice, Seynnes,..., Werkhausen (in preparation)

Cumulative Loading per step



No interaction effect (p = 0.246)

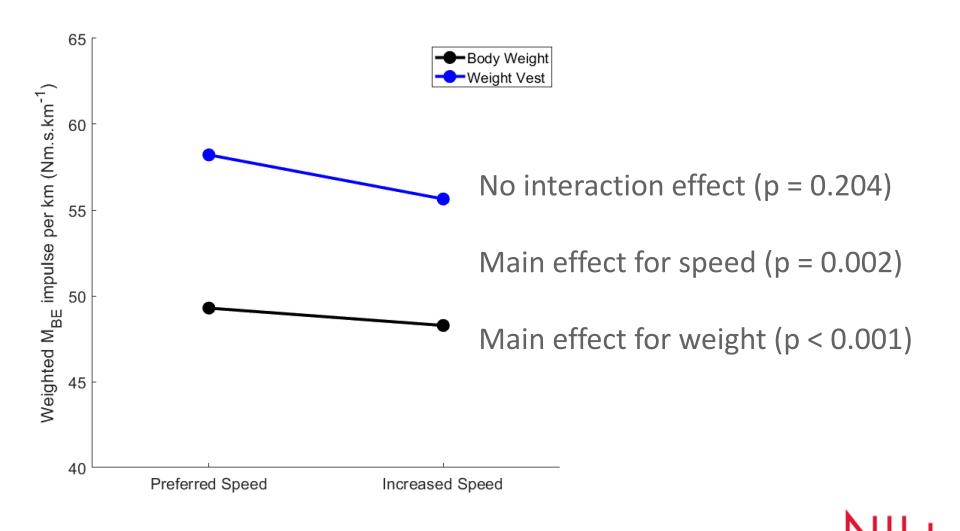
No main effect for speed (p = 0.166)

Main effect for weight (p < 0.001)



Rice, Seynnes,..., Werkhausen (in preparation)

Weighted Cumulative Loading per km



Rice, Seynnes,..., Werkhausen (in preparation)

Tibial stress during loaded running at two different speeds

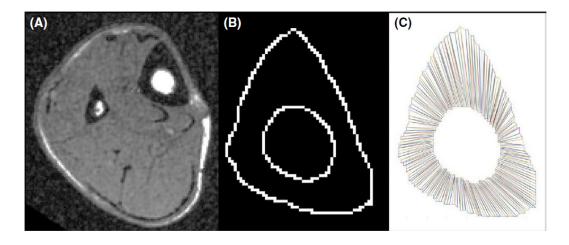
Increased running speed and weight carriage independently increase *peak* tibial loading

However, with increasing speed contact time decreases and fewer steps are required per distance

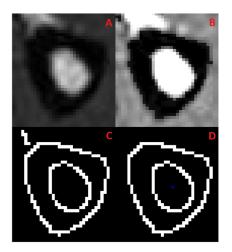
Therefore cumulative loading decreases per km with increasing speed, but is higher with greater weight carriage



Participant-specific estimates?



Rice et al., 2020







Ellison et al., 2020



Aim: to quantify second metatarsal stress during running when landing with a habitual rearfoot or non-rearfoot strike

Ellison et al., 2020





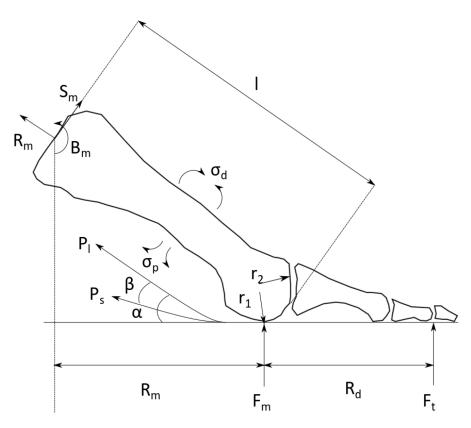


Barefoot running 3.6 m.s⁻¹ Synchronised motion capture and kinetics including RSscan plantar pressure plate MRI

Ellison et al., 2020





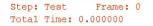


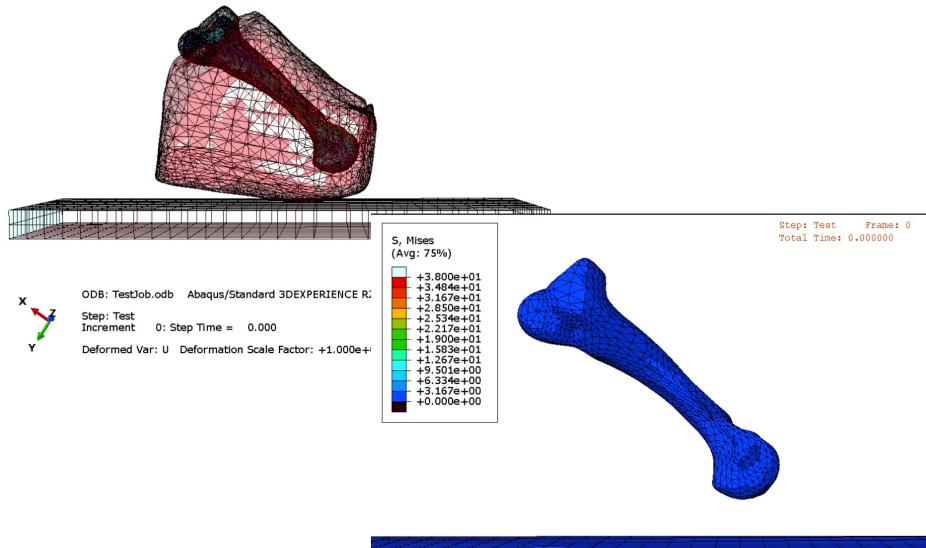
Similar peak stresses between groups despite greater peak external loading under the metatarsal head of nonrearfoot strikers

Ellison et al., 2020



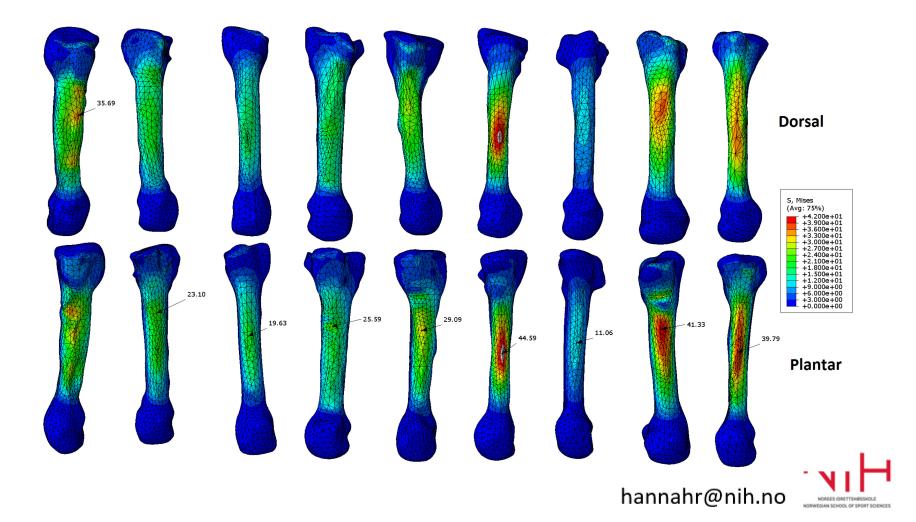




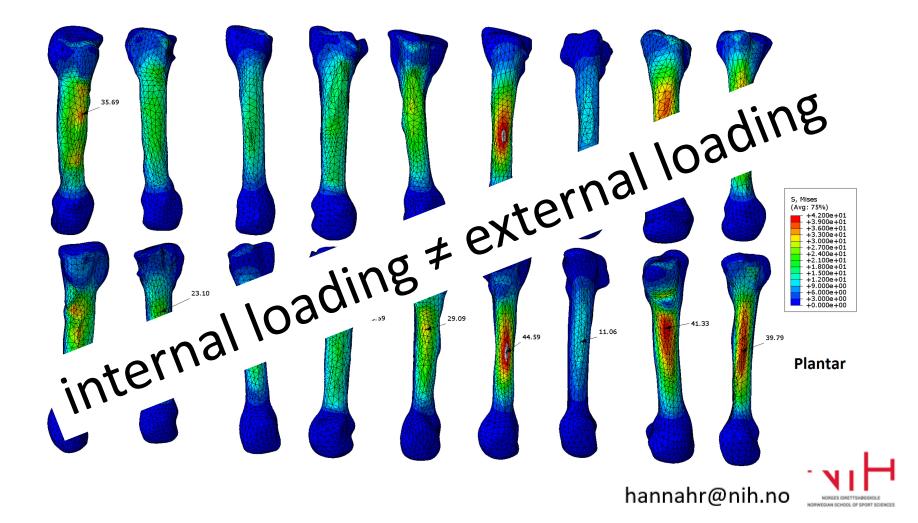


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Y		Prim	Increment 0: Step Time = 0.000 Primary Var: S, Mises Deformed Var: U Deformation Scale Factor: +1.000e+00																

No difference in maximum stress between rearfoot strikers and non-rearfoot strikers during running



No difference in maximum stress between rearfoot strikers and non-rearfoot strikers during running





Estimating Bone Loading in Real-time

- Robustness and validity of equipment to measure position, force, pressure...
- Real-time estimates of joint moments?
- Static optimisation time-consuming



Estimating Bone Loading in Real-time

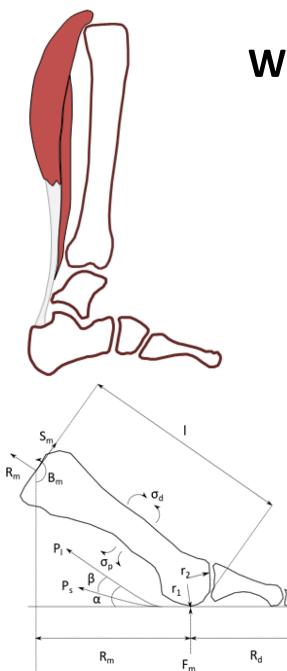
- Is CT/MRI required?
 - Participant-specific not needed to detect change in loading
- Can a simpler model be used?
 - Consider predictive modelling



Validation

- not truly validated
- comparison with strain gauge
- bone pin studies and direction of bending

Ultimately need injury outcomes

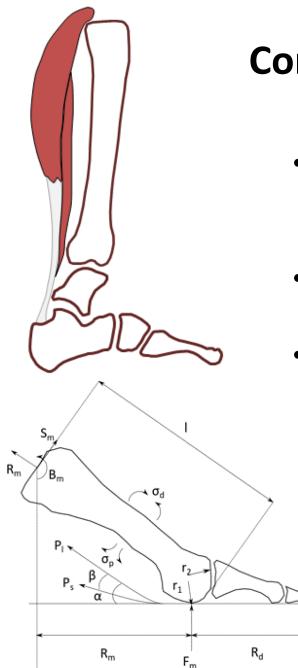


Where do we go next?

- Application to other movements
- Increasing ability to measure in-field
- Model improvement
 - Model validation

F,





Conclusions

- Exciting potential to quantify bone loading in-field, in real-time
- Implications for many
- Technology and modelling development is increasing at a fast pace

We need to understand it, not just measure it



Acknowledgements









Deutsche Sporthochschule Köln German Sport University Cologne





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Joe Hamill



Thank you!



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